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## Reliability of a Barre-Mounted Dynamometer-Stabilizing Device in Measuring Dance-Specific Muscle Performance

### Comments

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# 1 **The Reliability of a Barre-Mounted Dynamometer Stabilizing Device in Measuring** 2 **Dance Specific Muscle Performance**

3 Melissa Strzelinski, Lori Thein Brody, Jo Armour Smith, Shaw Bronner  
4

## 5 **ABSTRACT**

6 **Background:** Handheld dynamometry (HHD) is considered an efficient, effective, and  
7 portable means of objectively measuring lower extremity strength, however, it has yet to  
8 be studied specific to dance-relevant muscle performance. Furthermore, dynamometry  
9 is often criticized for variability in results based on tester strength and sex. Use of an  
10 external stabilizing device has been suggested to minimize differences in outcomes  
11 between male and female testers by reducing variability associated with tester strength  
12 limitations. Therefore, this study used a barre-mounted, portable dynamometer  
13 stabilizing device to improve consistency of results among different testers for  
14 assessing hip and lower extremity muscle performance in dance-relevant positions.

15 **Objective:** To assess the intra and inter-rater reliability of a barre-mounted  
16 dynamometer stabilizing device in measuring muscle performance in common dance  
17 maneuvers.

18 **Study Design:** Prospective Correlation Study

19 **Level of Evidence:** III

20 **Methods:** The primary investigator and a second tester assessed muscle performance  
21 of three common dance maneuvers: développé en avant, à la secondé, and arabesque,  
22 on 11 pre-professional and professional dancers on two separate occasions to establish  
23 intra- and inter-rater reliability of the barre-mounted dynamometer stabilizing device.

24 **Results:** Intra-rater reliability was moderate to high, and inter-rater reliability of the  
25 device was excellent, with Intra Class Correlation Coefficient values ranging from 0.527-  
26 0.851 and 0.834-0.953, respectively, for all positions. These results should be  
27 interpreted with caution, however, as these correlations are limited to two testers.

28 **Conclusions:** The barre-mounted stabilizing device shows promise in mitigating tester  
29 strength or fatigue in assessing the muscle performance of dancers. Initial assessment  
30 of the device suggests further study may be indicated to improve generalizability to

31 applications of larger scale muscle performance screening and assessment in dancers.  
32 or other athletic populations who engage in movements that require extensive hip range  
33 of motion and multi-joint stability.

34 **Clinical Relevance:** Using a portable, barre-mounted stabilizing device in assessing  
35 multi-joint lower extremity muscle performance in dancers improves consistency of  
36 testing results. Application of this testing device into wider scale screenings could assist  
37 in developing normative data for a population that is lacking. Broader applications to the  
38 upper extremity and other populations are possible.

39

40 **KEY\_WORDS:** Hip joint/\*physiology, muscle strength dynamometer/\*statistics &  
41 numerical data, dancing\*

## 42 INTRODUCTION

43  
44 The role of hip strength in various pain syndromes, impairments and athletic  
45 performance is extensively studied;<sup>1-4</sup> however, the hip strength demands necessary for  
46 dancing at a professional or elite level remain unclear. The reported overall lifetime  
47 injury incidence of dancers ranges between 42 to 97 percent.<sup>5-11</sup> Seemingly under-  
48 reported during a dancer's career, retired ballet dancers are 2.9 times more likely to  
49 report hip pain than non-dancers.<sup>12, 13</sup> Hip musculature provides dynamic stabilization  
50 and passive resistance to external forces. Axial loading combined with repetitive hip  
51 rotation without the prerequisite hip muscular performance is considered a potential  
52 precursor to hip pathology.<sup>3</sup> The repetitive nature of dance training, especially high  
53 frequency and volume external rotation, suggests the potential for injury to the  
54 capsulolabral and ligamentous structures of the hip joint associated with micro-instability  
55 is heightened.<sup>14, 15</sup> Appropriate hip muscle activation and strength are critical  
56 contributors to hip stability during dynamic movements of the lower extremity. At  
57 present, no study has quantified the strength required to sustain gesture limb position  
58 associated with the impressive aesthetics in dance.

59 Handheld dynamometry (HHD) is recognized as a reliable alternative to manual  
60 muscle testing for objective measurement of an individual's strength.<sup>16-19</sup> HHD provides  
61 a more cost-effective, efficient and portable means of assessing strength in a variety of  
62 clinical settings compared to isokinetic testing, the criterion standard for assessing  
63 muscle strength and performance.<sup>20</sup> Though more reliable and objective than traditional  
64 manual muscle testing, HHD is scrutinized for variability observed between testers of  
65 different sex and strength, as differences can exist in the tester's ability to stabilize the

66 HHD against repetitive force over time, or the tester's strength relative to the muscle  
67 group tested, particularly when assessing strong individuals (e.g. athletes).<sup>17, 21</sup> External  
68 stabilization of the HHD is suggested as a solution to reduce the influence of tester  
69 strength and the potential for systematic bias and large measurement variation across a  
70 study population.<sup>1, 2, 20, 22</sup> Nadler et al.<sup>2</sup> found an external anchoring device had excellent  
71 intra-rater reliability (ICC 0.94-0.98) in HHD measures of hip abduction and extension in  
72 collegiate athletes.

73         The purpose of this study was to assess the reliability of a barre-mounted  
74 dynamometer stabilizing device in evaluating muscle performance of dance-relevant  
75 positions. It was hypothesized that the stabilization device would be a reliable means of  
76 identifying mid-range muscle performance in dancers without hip pain. It was  
77 anticipated that test/re-test of muscle performance in dance-relevant positions with a  
78 barre-mounted stabilizing device would demonstrate consistency in results comparable  
79 to existing HHD reliability for both inter- and intra-rater reliability ( $r \geq 0.80$ ; excellent).

## 80 **METHODS**

### 81 Study subjects

82         Eleven participants (3 males, 8 females) were recruited from the <BLINDED>.  
83 Ballet professional and pre-professional companies and schools via flyers, email and  
84 word of mouth communication. An *a priori* power analysis suggested 9 participants  
85 would be necessary to demonstrate 0.80 power, with 0.05 alpha and effect size of  
86 0.70.<sup>23</sup> Participants were required to meet the following inclusion criteria: technical  
87 ability to hold *développé en avant*, *a la secondé* and *arabesque* at  $\geq 90$  degrees,  
88 currently dancing >20 hours per week, between 18-45 years of age, and available for

89 testing on two, separate occasions. Both male and female dancers were included.  
90 Participants were excluded if they had an acute lower extremity or hip muscle injury,  
91 acute radicular lumbar pathology (current L2-S1 myotomal weakness, sensory  
92 disturbances in the lower extremity), or were unable to perform lower extremity weight  
93 bearing due to existing injury.

94 The study was approved by the <BLINDED> Institutional Review Board (#  
95 <BLINDED>). Informed consent was obtained from all participants prior to enrollment in  
96 the study and all rights were protected.

#### 97 Procedures and Data Collection

98 The primary investigator and a second tester assessed 11 individuals in the  
99 dance-relevant positions described below. Both testers had over eight years of  
100 experience as physical therapists working with the dance population and underwent  
101 training to ensure testing was standardized.

102 On the initial visit, a pre-participation questionnaire, which included demographic  
103 information, dance training history and self-reported height/weight, was completed and  
104 informed consent was obtained. Participants completed a self-selected warm up as they  
105 would before a ballet technique class prior to testing. Tape was applied circumferentially  
106 around the right lower leg five centimeters above the superior aspect of the medial  
107 malleolus. Participants were instructed to establish contact of the tape to the  
108 dynamometer during testing to ensure consistency in force production lever arm across  
109 positions of relative hip flexion, abduction and extension. To avoid systematic bias,  
110 participants drew a card to determine which tester they began with. Test position order  
111 was randomized by card draw and recorded to allow for repeat testing on the second

112 day of data collection. Test positions were performed on the right side only to measure  
113 muscle performance of:

- 114 • *Développé en avant (front)*: Relative hip flexion and external rotation (participant  
115 behind stabilization device)
- 116 • *Développé a la secondé (side)*: Relative hip abduction and external rotation  
117 (participant beside stabilization device)
- 118 • *Développé arabesque (back)*: Relative hip extension and external rotation  
119 (participant in front of stabilization device)

120 The primary investigator attached the stabilization device to a wall-anchored,  
121 wooden ballet barre. A Hoggan Scientific, LLC. microFET®2 digital handheld  
122 dynamometer muscle tester was attached to the disc of the stabilization device with  
123 Velcro squares and an elastic band (Figure 1). The device used a carbon fiber pole  
124 running at an oblique angle from the barre to the wall to maximize stabilization against  
125 vertically directed force. Stackable blocks were used to bring the subject's hip angle to  
126 90° when necessary. The hip angle was assessed visually using the greater trochanter  
127 and lateral malleolus as reference points, and the standing leg as the vertical arm.  
128 Number of blocks were recorded to maintain consistency between the two days of data  
129 collection. The same studio and setup described above were completed on the second  
130 day of data collection.

131 Participants were instructed to use their normal degree of hip external rotation or  
132 turnout with full knee extension in each test position. Participants were allowed to  
133 stabilize with the hand closest to the barre during *développé en avant* and *arabesque*  
134 (Figures 2a and 2c), and rest both hands on the barre during *développé a la secondé*



135 (Figure 2b). Participants completed three trials of four to five seconds per test position.  
136 The testers used a scripted dialogue to minimize encouragement and maximize the  
137 force production: “Extend your leg in your normal turn out, and press into the  
138 dynamometer as hard as you can keeping your knee straight and hold, hold, hold, hold.”  
139 When necessary, the tester helped establish initial contact of the band of tape with the  
140 dynamometer.

141 An isometric “make” test was used to assess peak force production in développé  
142 en avant, a la secondé and arabesque of the right hip and lower extremity. A “make”  
143 test involves the subject exerting a maximal force against the dynamometer in a stable  
144 position, compared to a “break” test in which the examiner pushes the dynamometer  
145 against the subject’s limb until the subject’s maximal effort is overcome and the joint  
146 gives way.<sup>24</sup> Prior research has shown the “make” test produced more consistent  
147 magnitudes of force, contributing to higher observed reliability than “break” tests, where  
148 magnitudes were up to 1.3 times greater than “make” forces.<sup>24, 25</sup> The specific, dance-  
149 relevant positions selected are frequently executed and reflective of the characteristic  
150 tri-planar hip motion in dance.

151 Participants were allowed brief rest intervals of 30 to 60 seconds between test  
152 positions to allow for muscle recovery, and modification of block position to  
153 accommodate each new test position. Participants were given a break of at least 10  
154 minutes between testers to allow for muscle recovery. Repeat testing using the above  
155 protocol occurred at least one week but no more than two weeks following initial testing.  
156 All 11 participants returned for the second day of testing.

157 Data Analysis

158 Data was analyzed using IBM SPSS Statistics for Macintosh, Version 23.0 (IBM  
159 Corp. Released 2015. Armonk, NY). Data was evaluated for outliers and skewness and  
160 found to be normal. Descriptive statistics were calculated for baseline demographic  
161 information. HHD data was evaluated to determine Intraclass Correlation Coefficient  
162 (ICC) and 95% Confidence Intervals (CI) using a 2-way mixed model with absolute  
163 agreement for intra-rater reliability, and a 2-way random effects model with absolute  
164 agreement for inter-rater reliability (ICC 2,k).<sup>26</sup> ICC values range from 0.0 to 1.0, with  
165 values closer to 1.0 representing stronger reliability.<sup>27</sup> For the purpose of this study, ICC  
166 values were classified as follows: low  $\leq 0.49$ , moderate 0.50–0.69, high 0.70–0.89, and  
167 very high 0.90–1.00.<sup>28</sup> It should be noted that these values do not provide absolute  
168 standards; variability exists in reported levels of acceptance in the HHD literature. When  
169 interpreting ICC values, the clinician should be able to defend their classification of  
170 scoring based on the relative level of precision necessary in the observed  
171 measurements.<sup>27</sup>

172 The average of three trials per position was utilized for data analysis. The  
173 dynamometer measured force production in foot-pounds, which was converted to  
174 Newtons and normalized to participant weight (converted to Newtons by multiplying  
175 body weight in kilograms and the force of gravity) and height (meters) prior to data  
176 analysis. The formula used for normalization by weight and height was:  $d/(bw \cdot h) \times 100$   
177 where d = dynamometry means, bw = body weight and h = height in meters.  
178 Additionally, standard error of measurement (SEM) was calculated with 95%  
179 Confidence Interval (CI) as:

180 
$$SEM = SD [\sqrt{(1-r)}]$$

181  $95\% \text{ CI} = \text{observed score} \pm (1.96 \times \text{SEM})$

182 where SD = standard deviation of the set of observed test scores,  $r$  = the reliability  
183 coefficient for the measurement (ICC).<sup>27</sup> Calculating the SEM allows for estimation of  
184 the entire group, based on the established 95% confidence interval. For the purpose of  
185 the current study, the SEM provided the expected extent of error in different testers'  
186 scores for HHD.

## 187 **RESULTS**

188 Eleven participants (73% female) met all inclusion criteria, agreed to participate  
189 in the study, signed the informed consent, and completed all study parameters.

190 Participants had a mean age  $25.2 \pm 6.3$  years with  $18.5 \pm 6.9$  years total dance  
191 experience with the seven participants having  $9.71 \pm 5.43$  years of professional dance  
192 experience. Tables 1 and 2 provide demographic characteristics and mean values of  
193 the observed muscle force production for the reliability study population.

194 Intra-rater reliability ranged from moderate to high, with ICC values of 0.527-  
195 0.851 for Tester 1 and 0.531-0.692 for Tester 2 (Table 3). ICC values for arabesque had  
196 generally lower reliability and wider 95% confidence intervals. The SEM was generally  
197 low, and ranged from 0.077-0.527, with higher values observed for the arabesque  
198 position, suggesting a narrow range of measurement variability could be expected  
199 between testers and across positions.

200 Inter-rater reliability values were high to very high ( $>0.70$ ), with ICC values  
201 ranging from 0.834-0.953 (Table 4). SEM values for the average of three trials per  
202 position ranged from 0.034-0.322, with larger values observed for the arabesque  
203 position due to higher recorded force values in this position.

## 204 **DISCUSSION**

205 Inter-rater and intra-rater reliability of the barre-mounted dynamometer  
206 stabilizing device ranged from moderate to very high, supporting the utility of the device  
207 in assessing muscle performance in dance-relevant positions. It must be acknowledged  
208 that these results should be interpreted with caution due to the limited number of  
209 testers. The results are comparable to previous reports of intra-rater reliability of an  
210 external stabilizing device for HHD in an athletic population and do not differ from  
211 reported HHD reliability.<sup>1-3, 16, 17, 20, 22</sup> Scott et al. evaluated the use of a portable  
212 anchoring device for both inter- and intra-rater reliability, and against traditional HHD  
213 stabilization in measuring hip flexion, abduction and extension.<sup>1</sup> The authors reported  
214 comparable intra-rater reliability to the device in the current study, with ranges of 0.59-  
215 0.89 and 0.72-0.89, for a Tester A and B, respectively.<sup>1</sup> The authors also found the  
216 portable anchoring device yielded lower ICC values for hip extension, with a reported  
217 limitation of testing position, as the participants had difficulty securing contact with the  
218 device sensor in prone position.

219 The observed SEM values suggest a narrow interval of scoring would be  
220 anticipated with repeat assessment of dance-relevant position muscle performance  
221 though comparison to previous HHD reliability studies is limited. Thorborg et al.<sup>22</sup>  
222 reported values of 5-11% for SEM in evaluating the reliability of HHD with an external  
223 stabilization belt; however, HHD values were not normalized to height and mass. The  
224 HHD values in the current study were considerably lower than cardinal plane hip  
225 measures Thorborg et al.<sup>18</sup> reported in an athletic population, and likely account for the  
226 lower SEM values. Less force generation is possible when muscles are in their

227 shortened range at 90°. In the current study, arabesque accounted for the largest SEM,  
228 likely due to the increased force production capability of the dancers in this position and  
229 compensatory recruitment of trunk extensors, as mean values for arabesque were  
230 considerably higher than the other two positions.

231 This study approached a topic with minimal representation in the literature in  
232 attempting to identify a reliable means of assessing muscle performance in dancers.  
233 Despite the popularity of pre-participation screening in dance institutions across the  
234 United States, HHD is not typically included in this assessment, and therefore,  
235 normative values for HHD of cardinal plane hip strength in dancers have yet to be  
236 reported. Future studies may incorporate HHD to provide a basic understanding of the  
237 strength demands required of pre-professional and professional dancers.

#### 238 Limitations

239 The introduction of a barre-mounted dynamometer stabilization device is not  
240 without limitations. Dancer positioning was monitored to ensure the trunk remained  
241 vertical with light stabilization through the upper extremity to minimize potential  
242 compensatory force generation through the trunk and spine across test positions.  
243 However, it must be noted that contributions of the abdominals and erector spinae were  
244 possible.

245 This was most evident in the ability of two participants to overpower the lever arm  
246 stabilization of the device during the second day of data collection. This required  
247 additional stabilization by the tester to stop the device from rotating around the ballet  
248 barre against extreme force in développé arabesque. The wider confidence intervals  
249 and lower intra-rater reliability measures observed for arabesque could have arisen

250 from competitive bias, a learning effect, or a weakness of the device. The participants  
251 began trying to exceed the top known scores from initial testing despite the best efforts  
252 of the testers to keep individual results private. As previously mentioned, the lower  
253 reliability observed in this position could relate to compensatory lumbar lordosis or  
254 recruitment of back extensors versus true hip extension, yielding variability in results or  
255 change in limb position from leaning forward and losing contact with the dynamometer  
256 sensor during testing. The device was consequently modified with a vertical arm to the  
257 floor to promote improved stabilization against the larger forces generated in développé  
258 arabesque prior to integration in a larger study evaluating the influence of hip pain on  
259 muscle performance in dancers.

260         It must be acknowledged that this device was specifically designed to provide a  
261 measure of multiplanar hip muscle performance in in positions that have not previously  
262 been documented, rather than quantify isolated hip muscle performance. This may be  
263 viewed as a potential limitation of the device. However, weakness in a functional  
264 position involving multiple joints could prompt further testing of the individual, synergistic  
265 muscles contributing to the motion to identify where the weakness exists. Future  
266 iterations of the study may benefit from shortening the lever arm of force application to  
267 the distal thigh to eliminate potential of full body compensation during dance specific  
268 maneuvers, or testing at each individual's true mid-range of motion.

269         Lastly, it should be recognized that the two testers in this study are expert  
270 clinicians, and further research across a wider variety of testers would be helpful to  
271 improve the generalizability of the results to inexperienced clinicians.

272           This study was the first of its kind in two ways specific to the dance population:  
273 assessing muscle performance in dance-relevant positions and using a barre-mounted  
274 dynamometer stabilizing device that can be used within the dance studio. The integrity  
275 of the ballet barre or anchoring point for the stabilization device itself could arise as a  
276 limitation. The current study included a wall-anchored, rigid ballet barre that did not flex  
277 under pressure.

278           While the positions selected are completed at high frequency in both technique  
279 classes and rehearsals, it is not known if these are the most representative of the  
280 strength demands for sustaining gesture limb positions. Use of surface  
281 electromyography (EMG) could better inform muscle firing patterns required for each  
282 movement; however, this was beyond the scope of the current study. The novel design  
283 of the stabilization device provides an efficient, cost-effective and portable means of  
284 better understanding the unique strength demands dance requires.

## 285 **CONCLUSION**

286           The observed findings suggest muscle performance of dance specific maneuvers  
287 of *développé en avant* and *a la secondé* can be reliably measured with a barre-mounted  
288 dynamometer stabilizing device. The device is easily portable and can be easily  
289 adjusted to accommodate ballet barres of variable diameters. Further investigation of an  
290 improved means of stabilization for *développé arabesque* should be considered to  
291 improve reliability. The device may have broader applicability in the genre of athletes  
292 such as figure skaters and gymnasts who require positions and maneuvers requiring a  
293 larger range of hip motion and multi-joint stability. The device has value in eliminating  
294 differences in strength among testers, particularly when the device could be integrated

295 into pre-participation screenings and testing across different geographic locations. The  
296 device has potential utility in the general population, as it could be anchored to a railing  
297 or parallel bars in a standard physical therapy clinic setting.

298 Broader applications of this device may help establish normalized data for dance  
299 specific muscle performance measures, and potentially be used to identify strength  
300 impairments in the dance population. Future research efforts may focus on  
301 modifications to the original device to allow for greater generalizability and adaptability  
302 in measuring both upper and lower extremity muscle force production and incorporating  
303 the use of surface EMG during dance specific movements to improve our understanding  
304 of the muscle activation required for the physical demands dance requires.



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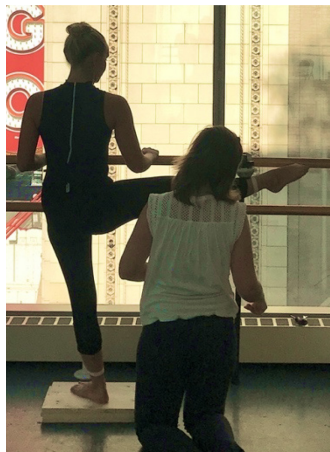
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396 **Figure 1: Study Equipment**

405 **FIGURE 1a-b:** DynaRail anchoring system and Hoggan Scientific, LLC. microFET®2 digital handheld  
 406 dynamometer muscle tester. The dynamometer is attached to the disc device with Velcro squares and  
 407 elastic band.  
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a



b



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412 **Figures 2a-2c Test positions:**2a) Développé en avant (front); 2b) Développé à la seconde (side);  
 413 2c)

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**Figure 4:** Test position for développé arabesque (back).

440 **TABLE 1: Study Demographics**

	<b>Female</b>	<b>Male</b>	<b>Total</b>
Participants (%)*	8 (72.7%)	3 (27.3%)	11 (100%)
Professional dancers (%)	5 (45.5%)	2 (18.2%)	7 (63.7%)
Pre-Professional/Student (%)	3 (27.3%)	1 (9.1%)	4 (36.4%)
Age (yrs)	24.0 ± 5.43	28.33 ± 8.51	25.2 ± 6.30
Dance training (yrs)	18.13 ± 6.79	19.33 ± 8.62	18.45 ± 6.89
Professional experience (yrs) <sup>†</sup>	8.50 ± 5.36	12.75 ± 6.01	9.71 ± 5.43
Weight (kg)	51.48 ± 4.33	66.53 ± 3.46	55.6 ± 8.06
Height (m)	1.65 ± 0.06	1.72 ± 0.02	1.67 ± 0.06

441 \*All percentages are given as % of the total. Abbreviations: yrs=years, m=meters, kg=kilograms.

442 <sup>†</sup>Mean of 7 subjects with professional experience.

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445 **TABLE 2: Mean muscle force production by Day, Position and Tester**

	Day 1: Mean±SD	Day 2: Mean±SD
<i>Développé en avant/Front</i>		
Tester 1	1.102 ± 0.293	1.292 ± 0.401
Tester 2	1.106 ± 0.273	1.338 ± 0.360
<i>Développé a la seconde/Side</i>		
Tester 1	1.135 ± 0.383	1.408 ± 0.442
Tester 2	1.101 ± 0.246	1.390 ± 0.437
<i>Développé arabesque/Back</i>		
Tester 1	2.303 ± 0.724	3.628 ± 1.155
Tester 2	2.333 ± 0.823	3.637 ± 0.762

446 *Isometric muscle force production (Nm) was normalized by body weight (N) x height (m) x 100; SD = Standard*447 *Deviation*

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450 **TABLE 3: Intra-rater Reliability by Position and Tester**

<b>Intra-rater Reliability</b>	<b>ICC (95% CI)</b>	<b>SEM</b>
<i>Développé en avant/Front</i>		
Tester 1	0.851 (0.177 - 0.964)	0.077
Tester 2	0.692 (-0.096 - 0.917)	0.148
<i>Développé a la seconde/Side</i>		
Tester 1	0.739 (-0.006 - 0.931)	0.164
Tester 2	0.624 (-0.197 - 0.895)	0.198
<i>Développé arabesque/Back</i>		
Tester 1	0.527 (-0.240 - 0.870)	0.527
Tester 2	0.531 (-0.104 - 0.881)	0.302

451 *ICC = r value (intraclass correlation coefficient); CI=Confidence Interval; SEM = Standard Error of Measurement.*  
 452 *Isometric muscle force production (Nm) was normalized by body weight (N) x height (m) x 100.*

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454 **TABLE 4: Inter-rater Reliability by Position and Day**

<b>Inter-rater Reliability</b>	<b>ICC (95% CI)</b>	<b>SEM</b>
<i>Développé en avant/Front</i>		
Day 1	0.843 (0.391 - 0.958)	0.085
Day 2	0.954 (0.838 - 0.988)	0.034
<i>Développé a la seconde/Side</i>		
Day 1	0.834 (0.371 - 0.956)	0.102
Day 2	0.953 (0.823 - 0.987)	0.042
<i>Développé arabesque/Back</i>		
Day 1	0.858 (0.454 - 0.962)	0.213
Day 2	0.828 (0.329 - 0.954)	0.322

455 *ICC = r value (intraclass correlation coefficient); CI=Confidence Interval; SEM = Standard Error of Measurement.*  
 456 *Isometric muscle force production (Nm) was normalized by body weight (N) x height (m) x 100.*

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